Optimal Basis Function Study in Wavelet Sample Entropy for Electrical Cardioversion Outcome Prediction of Persistent Atrial Fibrillation

R Alcaraz¹, JJ Rieta², A Martínez¹

¹Innovation in Bioengineering Research Group. University of Castilla-La Mancha, Cuenca, Spain ²Biomedical Synergy, Electronic Engineering Dept., Universidad Politécnica de Valencia, Spain

Abstract

Wavelet Sample Entropy (WSE) has been previously introduced as a successful methodology to predict electrical cardioversion (ECV) outcome of persistent atrial fibrillation (AF). The method estimates AF organization based on the combination of Wavelet decomposition and a nonlinear regularity metric, such as Sample Entropy (SampEn). However, WSE has been only computed by applying a specific wavelet function, such as the fourth-order biorthogonal wavelet. In the present work, with the objective of improving WSE robustness and its diagnostic ability in ECV outcome prediction, several orthogonal wavelet families were tested, and their performances were compared. Results indicated that, for all the functions of the same wavelet family, the same sensitivity and specificity values were obtained. Additionally, all the wavelet families reached the same diagnostic ability (80.95% sensitivity and 85.71% specificity), the same patients being incorrectly classified by all the families. These results suggest that any wavelet function could be indistinctly used to estimate successfully AF organization with the WSE methodology. As a consequence, the design of a customized wavelet function adapted to the specific characteristics of AA would not improve the WSE diagnostic ability in the prediction of ECV outcome in AF.

1. Introduction

For patients in persistent atrial fibrillation (AF), restoration and maintenance of normal sinus rhythm (NSR) is the main therapeutic goal because symptoms, cardiac output, and exercise tolerance are improved whereas the risk of stroke is reduced [1]. Thus, the first step in the rhythm control strategy is generally cardioversion. While chemical-induced cardioversion is sometimes possible, particularly with amiodarone [2], it is generally more unsuccessful than electrical cardioversion (ECV), specially if the arrhythmia has been present for more than 24 hours [2]. However, although the ECV success rate is high, AF recurrence is

common, especially during the first 2 weeks following the procedure [3]. Moreover, ECV also has the potential of causing severe collateral effects, such as post-shock bradycardia, malignant ventricular arrhythmias, arterial thromboembolism and complications related to anaesthesia [2]. Hence, it would be clinically very useful to predict NSR maintenance after ECV, before it is attempted. In this way, the risks of cardioversion could be avoided for those patients with high risk of short-term recurrence and, for the health care provider, clinical costs could be optimized because unproductive treatment time and bed usage could be reduced.

To this respect, a strategy called Wavelet Sample Entropy (WSE) has been recently introduced as a successful methodology to predict ECV outcome [4]. The method estimates AF organization based on the combination of Wavelet decomposition and a non-linear regularity metric, such as Sample Entropy (SampEn), showing that in patients with a more organized AF, the arrhythmia recurrence likelihood was lower after ECV [4]. However, WSE was only computed by applying a specific wavelet function, such as the fourth-order biorthogonal wavelet. Thereby, in the present work, with the objective of improving WSE robustness and its diagnostic ability in ECV outcome prediction, several orthogonal wavelet families were tested, and their performances were compared.

2. Materials

2.1. Study population

Thirty-five patients (12 men and 23 women) with persistent AF lasting more than 30 days, undergoing ECV were followed during four weeks. All patients were in drug treatment with amiodarone. A standard 12-lead ECG was acquired prior to cardioversion. All signals were digitized at a sampling rate of 1024 Hz and 16-bit resolution with a Cardiolab System in the electrophysiology laboratory during ECV protocol. In order to process these signals, a 30 seconds-length AF segment preceding the ECV was extracted for each patient. After the ECV, in 21 pa-

tients (60%) NSR duration was below one month, whereas in the remaining 14 (40%) NSR was maintained.

2.2. Data preprocessing

Lead V_1 was chosen for the analysis because previous works have shown that atrial activity (AA) is dominant in this lead [5]. The signal was preprocessed in order to improve later analysis. Firstly, baseline wander was removed making use of bidirectional high pass filtering with 0.5 Hz cut-off frequency [6]. Secondly, high frequency noise was reduced with an eight-order bidirectional IIR Chebyshev low pass filtering, whose cut-off frequency was 70 Hz [7]. Finally, powerline interference was removed through adaptive notch filtering, which preserves the ECG spectral information [8].

3. Methods

3.1. Wavelet sample entropy

The WSE methodology has shown an ability to detect regularity variations in the AA signal that would be left masked in other cases [4]. However, this strategy requires the combination of Wavelet decomposition and SampEn together with some additional steps, such as it will be next described.

The analysis of the AA from the surface ECG is complicated by the simultaneous presence of ventricular activity, which is of much greater amplitude. Whereby, the AA signal has to be firstly extracted before the application of any other analysis. Although a variety of different techniques exist for this purpose, a QRST cancellation method was used. Thus, the highest variance eigenvector of all the ECG beats was considered as the ventricular template for the cancellation. This QRST template was selected because it was able to obtain a more accurate ventricular activity representation and, hence, higher quality AA extraction in short AF recordings, such as the analyzed in this work, than those obtained by averaging all the beats [9].

Next, eight levels of wavelet decomposition were applied to the AA signals because the seventh detail scale (sub-band corresponding to 4–8 Hz) covers the most typical AA frequency range [10]. The wavelet coefficients vector corresponding to the scale containing the dominant atrial frequency, those with the largest amplitude within the AA frequency range [10], was linearly interpolated by the factor 2^{m-1} , being m the discrete wavelet scale. Hence, a vector of wavelet coefficients with a number of samples equal to the original signal was obtained for the chosen scale. Considering that different scales present wavelet coefficients vectors with different number of samples, this interpolation was necessary. Moreover, unsuccessful results were obtained when non-interpolated wavelet coefficients

vectors were analyzed. Finally, the regularity of this vector was estimated making use of SampEn to discern between ECVs relapsing to AF and resulting in NSR.

3.2. Sample entropy

Sample Entropy (SampEn) examines a time series for similar epochs and assigns a non-negative number to the sequence, with larger values corresponding to more complexity or irregularity in the data [11]. Two input parameters, a run length m and a tolerance window r, must be specified for SampEn to be computed. SampEn(m,r) is the negative logarithm of the conditional probability that two sequences similar during m points remain similar at the next point, where self-matches are not included in calculating the probability. A detailed mathematic description can be found in [11].

Although m and r are critical in determining the outcome of SampEn, no guidelines exist for optimizing their values. Nevertheless, the most widely used values are those suggested by Pincus, i. e. m=1 or m=2 and r between 0.1 and 0.25 times the standard deviation of the original time serie [12]. Hence, considering that previous works, where SampEn was also applied to AF signals, reported the best results with m=2 and r=0.25 times the standard deviation of the data [4,13,14], these values were selected for the present study.

3.3. Optimal wavelet function study

Given that there are no established rules for the choice of a specific wavelet family for each particular application, several orthogonal wavelet families were tested in this work. Only experiments with orthogonal families were developed because only in an orthogonal basis any signal can be uniquely decomposed and the decomposition can be inverted without loosing information [15]. Concretely, all the different functions from Haar, Daubechies, Coiflet, Biorthogonal, Reverse Biorthogonal and Symlet wavelet families were tested.

3.4. Statistical analysis

Obtained SampEn values were expressed as mean \pm standard deviation, because ECVs relapsing to AF and resulting in NSR had a normal and homoscedastic distribution as the Kolmogorov–Smirnov and Levene tests proved, respectively. Thereby, the Student's t-test was also used to determine whether there was any significant difference between the groups. A two-tailed value of p<0.05 was considered statistically significant.

In order to evaluate the predictive ability of the WSE for the NSR maintenance with each wavelet function, a

receiver operating characteristic (ROC) curve was constructed. Different thresholds or cutoff points (SampEn values) were selected and the sensitivity/specificity pair for each one of them was calculated. Sensitivity (the true positive rate) was considered as the ECVs relapsing to AF proportion correctly classified (SampEn value higher than the cutoff point), whereas specificity (the true negative rate) represented the ECVs resulting in NSR percentage correctly recognized (SampEn value lower than the cutoff point). The closest point to 100% sensitivity and specificity was selected as optimum SampEn threshold.

4. Results

For all the functions of the same wavelet family, the same sensitivity and specificity values were obtained. Thereby, only the function that showed lower p value is presented in Table 1 for each wavelet family. As can be appreciated in the table, all the wavelet families reached the same efficiency, i.e. a sensitivity of 80.95% (17 out of 21) and a specificity of 85.71% (12 out of 14), the same patients being incorrectly classified by all the families. Additionally, for all the cases, the ROC curves provided an optimum SampEn discrimination threshold between 0.029 and 0.030. Similarly, for all the wavelet families, the patients relapsing to AF presented higher SampEn values than those resulting in NSR after one month, and both groups were statistically distinguishable, since a statistical significance lower than 0.001 was obtained. In this sense, Figure 1 shows, as an example, the ROC curve and the classification into patients resulting in NSR and relapsing to AF obtained with the third-order Coiflet family.

5. Discussion and conclusions

The wavelet coefficients vector SampEn analysis checks the regularity of a time series. This time series is constituted by the correlation coefficients between the scaled mother wavelet and consecutive and non-overlapping signal segments. In this respect, results provided by all the tested wavelet families can be considered as coherent and prove that the discrete Wavelet transform translation variance has no effect in this application. Additionally, a high regularity value in this time series indicates constant waveform across the studied time period. On the contrary, low regularity implies variable waveforms. Thus, the presence of more structured f waves in organized atrial activities [5] could justify the obtained results, which show that patients who relapsed to AF presented lower wavelet coefficients vector regularity than those who remained in NSR. Hence, it could be considered that WSE is able to obtain a successful AF organization estimation independently of the selected wavelet function.

Finally, the obtained results also suggest that the design

of a customized wavelet function adapted to the atrial activity waveform characteristics would not considerably improve the prediction of ECV result. In fact, in other studies, where different ECG problems were solved making use of Wavelet transform, a new wavelet function adapted to the analyzed signal characteristics was considered but, finally, discarded [16].

Acknowledgements

This work was supported by the projects TEC2007-64884 from the Spanish Ministry of Science and Innovation, PII2C09-0224-5983 and PII1C09-0036-3237 from Junta de Comunidades de Castilla La Mancha and PAID-05-08 from Universidad Politécnica de Valencia.

References

- [1] Fuster V, Rydén LE, Cannom DS, Crijns HJ, Curtis AB, Ellenbogen KA, et. al. ACC/AHA/ESC 2006 guidelines for the management of patients with atrial fibrillation: a report of the American College of Cardiology/American Heart Association task force on practice guidelines and the european society of cardiology committee for practice guidelines (writing committee to revise the 2001 guidelines for the management of patients with atrial fibrillation): developed in collaboration with the european heart rhythm association and the heart rhythm society. Circulation Aug 2006; 114(7):e257–e354.
- [2] Gall NP, Murgatroyd FD. Electrical cardioversion for AFthe state of the art. Pacing Clin Electrophysiol Apr 2007; 30(4):554–567.
- [3] Tieleman RG, Gelder ICV, Crijns HJ, Kam PJD, Berg MPVD, Haaksma J, Woude HJVD, Allessie MA. Early recurrences of atrial fibrillation after electrical cardioversion: a result of fibrillation-induced electrical remodeling of the atria? J Am Coll Cardiol Jan 1998;31(1):167–173.
- [4] Alcaraz R, Rieta JJ. Predicting electrical cardioversion outcome from surface ECG recordings through Wavelet Sample Entropy. Conf Proc IEEE Comput Cardiol 2008;1041– 1044.
- [5] Petrutiu S, Ng J, Nijm GM, Al-Angari H, Swiryn S, Sahakian AV. Atrial fibrillation and waveform characterization. A time domain perspective in the surface ECG. IEEE Eng Med Biol Mag 2006;25(6):24–30.
- [6] Dotsinsky I, Stoyanov T. Optimization of bi-directional digital filtering for drift suppression in electrocardiogram signals. J Med Eng Technol 2004;28(4):178–180.
- [7] Sun Y, Chan K, Krishnan SM. ECG signal conditioning by morphological filtering. Comput Biol Med Nov 2002; 32(6):465–479.
- [8] Ferdjallah M, Barr RE. Adaptive digital notch filter design on the unit circle for the removal of powerline noise from biomedical signals. IEEE Trans Biomed Eng Jun 1994; 41(6):529–536.
- [9] Alcaraz R, Rieta JJ. Adaptive singular value QRST cancellation for the analysis of short single lead atrial fibrillation

Wavelet family (order)	ECVs relapsing AF	ECVs maintaining NSR	p-value	Sensitivity (%)	Specificity (%)
Haar	0.030 ± 0.006	0.026 ± 0.005	0.0100	80.95 (17/21)	85.71 (12/14)
Daubechies (5)	0.031 ± 0.006	0.027 ± 0.006	0.0112	80.95 (17/21)	85.71 (12/14)
Coiflet (3)	0.030 ± 0.007	0.025 ± 0.006	0.0098	80.95 (17/21)	85.71 (12/14)
Biorthogonal (4.4)	0.032 ± 0.005	0.027 ± 0.004	0.0072	80.95 (17/21)	85.71 (12/14)
Reverse Biorthogonal (4.4)	0.033 ± 0.006	0.029 ± 0.004	0.0115	80.95 (17/21)	85.71 (12/14)
Symlets (5)	0.031 ± 0.006	0.026 ± 0.005	0.0086	80.95 (17/21)	85.71 (12/14)

Table 1. Mean and standard deviation SampEn values for ECVs relaping to AF and resulting in NSR, statistical significance (p value), sensitivity and specificity for each tested wavelet family.

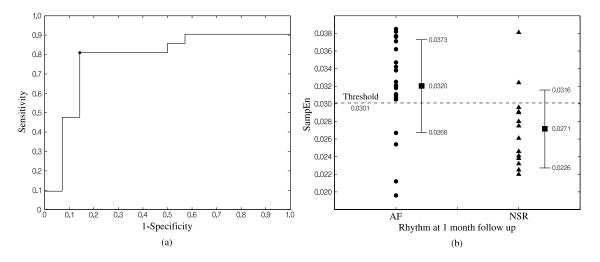


Figure 1. Results obtained with the third-order Coiflet wavelet family. (a) ROC curve constructed with the obtained SampEn values for persistent AF patients. The closest point to 100% sensitivity and specificity is selected as optimum SampEn threshold. Symbol • indicates the optimum threshold. (b) Classification into patients resulting in NSR and relapsing to AF after 4 weeks following ECV.

- electrocardiograms. Proc Comput Cardiol 2007;34:513–516.
- [10] Bollmann A, Husser D, Mainardi L, Lombardi F, Langley P, Murray A, Rieta JJ, Millet J, Olsson SB, Stridh M, Sörnmo L. Analysis of surface electrocardiograms in atrial fibrillation: techniques, research, and clinical applications. Europace Nov 2006;8(11):911–926.
- [11] Richman JS, Moorman JR. Physiological time-series analysis using approximate entropy and sample entropy. Am J Physiol Heart Circ Physiol Jun 2000;278(6):H2039–H2049.
- [12] Pincus SM. Approximate entropy as a measure of system complexity. Proc Natl Acad Sci U S A Mar 1991; 88(6):2297–2301.
- [13] Alcaraz R, Rieta JJ. Wavelet bidomain sample entropy analysis to predict spontaneous termination of atrial fibrillation. Physiol Meas Jan 2008;29(1):65–80.

- [14] Alcaraz R, Rieta JJ, Hornero F. Atrial activity non-invasive characterization in previous instants before paroxysmal atrial fibrillation termination. Rev Esp Cardiol Feb 2008; 61(2):154–160.
- [15] Mallat S. A Wavelet Tour of Signal Processing. Academic Press, 1999. ISBN 0-12-466606-X.
- [16] Addison PS. Wavelet transforms and the ECG: a review. Physiol Meas Oct 2005;26(5):R155–R199.

Address for correspondence:

Raúl Alcaraz Martínez
E. U. Politécnica de Cuenca
Campus Universitario
16071 Cuenca (Spain)
raul.alcaraz@uclm.es