

A New Delayless Sub-band Filtering Method for Cancelling the Effect of Feedback Path in Hearing Aid Systems

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Abstract— Various methods have been proposed to overcome the problem of compensating the acoustic feedback path that negatively impacts the performance of hearing aid devices. However, in most of them feedback path model is assumed to be fixed which is not quite realistic. In this paper, we consider fixed and variable feedback paths and analyze for each case the performance of one of the robust Adaptive Feedback Cancellation (AFC) schemes, i.e. the Prediction Error Method AFC which uses Partitioned Block Frequency-Domain Normalized Least Mean Square (Pbfd- NLMS) algorithm. Based on the analysis results we propose varying the step size values for the same adaptive algorithm on the fly by monitoring the misalignment criteria. The experimental results using the proposed method show improvement made on the system performance.

I. INTRODUCTION

In the current hearing aids, presence of acoustic feedback between loudspeaker and microphone causes some howling and whistling sound effects when the gain is increased in the forward path (Fig.1). Hence, Maximum Stable Gain (MSG) in the forward path is restricted by the acoustic feedback effect.

AFC is commonly used to reduce this negative effect. Fig. 1 shows the structure of a simple AFC. However, presence of the closed loop in this figure causes correlation between desired and feedback signals when the desired signal is a colored signal such as a speech signal. This correlation produces some amount of bias or error in the estimated coefficients of adaptive filter [1].

Different methods have been used to overcome this drawback and increase the precision of the AFC system. Prediction Error Method AFC (PEM-AFC) is a very successful method in this area in which whitening technique is performed to reduce the correlation between desired signal and feedback signal [1], [2]. This method consists of two adaptive procedures; one adaptively whitens the signal while the other one adaptively estimates the coefficients of the feedback path (Fig.2). Various methods can be used for mentioned adaptive filters [1], [3], and [4].

However, the majority of the proposed methods assume stationary feedback path while in practice the feedback path can change dynamically. In this paper, the method of PEM-AFC with Pbfd-NLMS is analyzed assuming dynamic feedback path. The algorithm is briefly described and its performance for static and dynamic feedback paths is compared. Based on the analysis results we propose adjusting the step size values for the same adaptive algorithm by monitoring

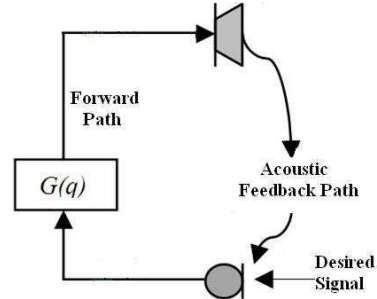


Fig. 1. Typical AFC algorithm

the misalignment criteria. The experimental results using the proposed method show improvement made on the system performance. The paper is organized as follows. Section II reviews PEM-AFC algorithm using Levinson-Durbin algorithm for whitening. Adaptive filter using Pbfd-NLMS for estimating of feedback path coefficients is explained in section III. Experimental results are presented in section IV and section V is the conclusion.

II. PEM-AFC

Common AFC algorithm suffers from bias in the estimated filter coefficients. Furthermore, correlation between desired signal and feedback signal causes some distortion in the processed signal.

PEM-AFC method (depicted in Fig. 2) reduces the correlation between these two signals and consequently lessens the amount of bias by means of whitening filters. This method, as it is shown in Fig.2, assumes that the desired signal $x[n]$ can be modeled by an AR process [1]:

$$x[n] = H(q, n)w[n] \quad (1)$$

Where $H(q, n)$ is an AR model and $w[n]$ is an impulse train or a zero-mean white noise sequence if the desired signal is voiced or unvoiced, respectively.

In Eq. 1, n and q^{-1} denote discrete-time index and discrete-time delay, respectively. $H(q, n)$ is a discrete-time FIR filter of length L which is a notation for:

$$H(q, n) = \mathbf{h}^T [n] \mathbf{q} \quad (2)$$

Where $\mathbf{h}[n] = [h_0[n] \ h_1[n] \ \dots \ h_{L_F-1}[n]]^T$ is the vector of the filter coefficients and $\mathbf{q} = [1 \ q^{-1} \ \dots \ q^{-L_F+1}]^T$.

Then filtering of $w[n]$ by $H(q, n)$ can be represented by any of these two notations:

$$H(q, n)w[n] = \mathbf{h}^T \mathbf{w}[n] \quad (3)$$

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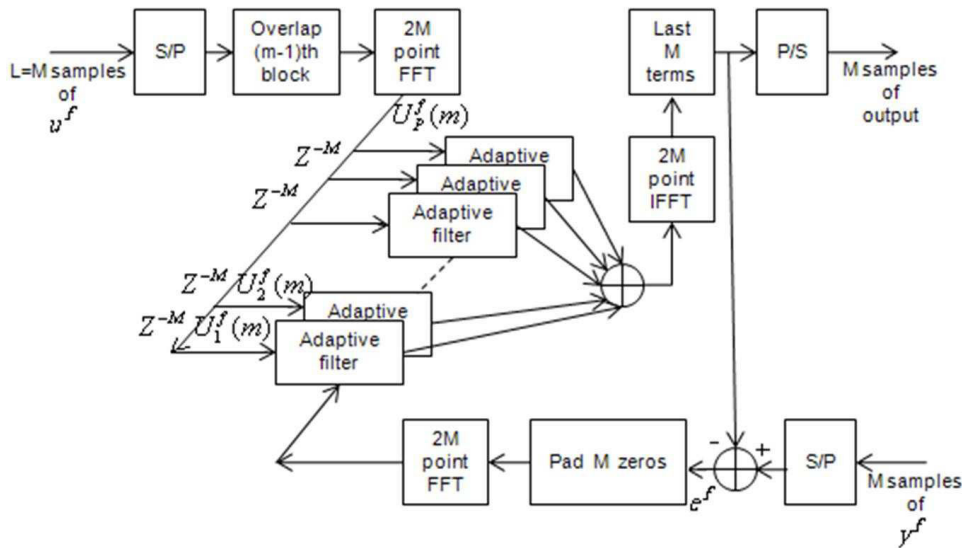


Fig. 3. PBFD-NLMS block diagram

5 and 6 are for two experiments differing only in the type of feedback path used. As seen in Fig. 6, for dynamic (varying) feedback path larger μ_0 values better. That is, for very small $\mu_0 = 0.0005$ the adaptive algorithm does not converge, or even if it does converge for some small value like $\mu_0 = 0.005$, still the system output shows howling and whistling effects. Conversely, large values (i.e. $\mu_0 = 0.1, 0.05$) make algorithm to track feedback changes better and faster. Focusing on Figs. 5 and 6, we see that smaller μ_0 is more suitable for the first part of the curves in which the system is stationary, then larger μ_0 is more desirable when the feedback path starts to change. As a result, selecting a variable μ_0 value based on the behavior of the misalignment seems to be the best approach. Therefore in our approach, we let the adaptive algorithm starts with a small μ_0 value (e.g. $\mu = 0.0005$) while monitoring the misalignment. If the misalignment has a noticeable increase (e.g. above a prescribed threshold level), system will recognize it as a change of the feedback path and will increase the μ_0 value (e.g. to $\mu = 0.1$). On the other hand, if misalignment amount goes less than a threshold level (e.g. $-3dB$), it would indicate that the system has been successful in tracking the feedback path changes and thus, smaller μ_0 will be chosen to further decrease the error and improve the misalignment even further if possible. That is, μ_0 value is gradually decreased depending on the behavior of the misalignment. Fig. 7 shows the results of our approach.

Moreover, subjectively comparison of the results shows more than 14% improvement in Perceptual Evaluation of Speech Quality (PESQ) of the output signal when variable μ_0 is used. That is, by implementing our approach, the quality of processed signal increases for the listener, i.e for the Hearing Aid user.

V. CONCLUSION

PBFD-NLMS method based on the partitioned convolutions has been used as a feedback canceller in

hearing aid. Static (fixed) and dynamic (varying) feedback models have been used to compare the performance of this algorithm. Our experimental results show that larger μ_0 is required to track dynamic changes of the feedback path. Thus, we have proposed replacing μ_0 in the PBFD-NLMS method by a misalignment-dependent variable step size. Simulation results confirm obtaining significant improvement in fast cancellation of the varying feedback path and in the performance of Hearing Aid device using our proposed approach.

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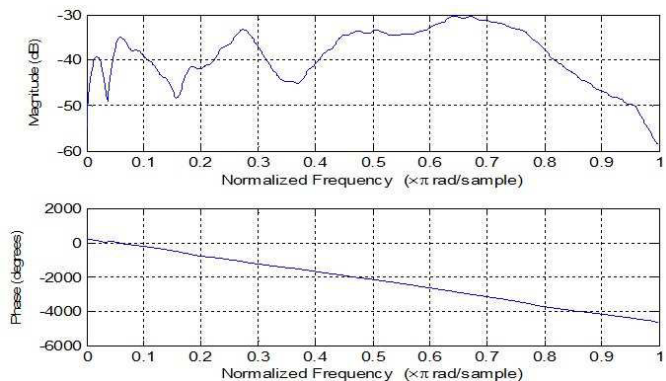


Fig. 4. Feedback Path Transfer Function

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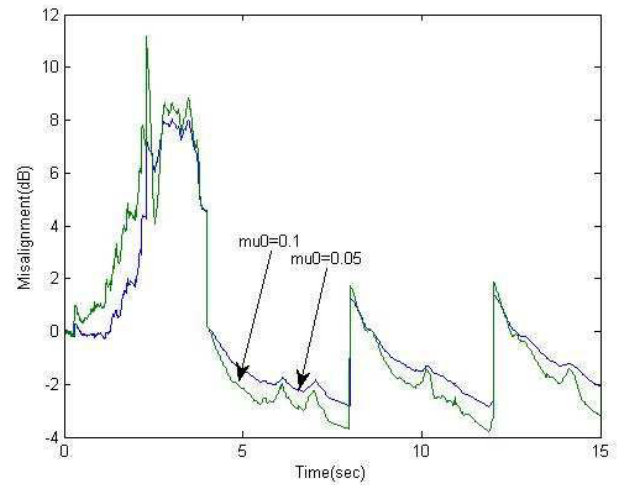


Fig. 6. Misalignment of PBFD-NLMS with dynamic (varying) feedback path using different step size values. The results are the average of 40 executions in each of which the initial feedback path is the one depicted in Fig. 4 and the other feedback models are randomly generated.

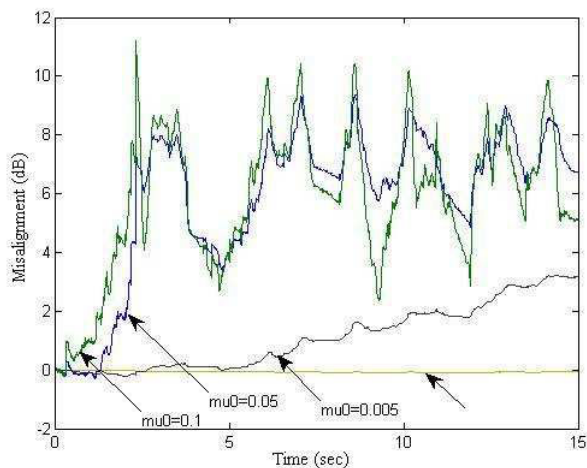


Fig. 5. Misalignment of PBFD-NLMS with static (fixed) feedback path using different step size values

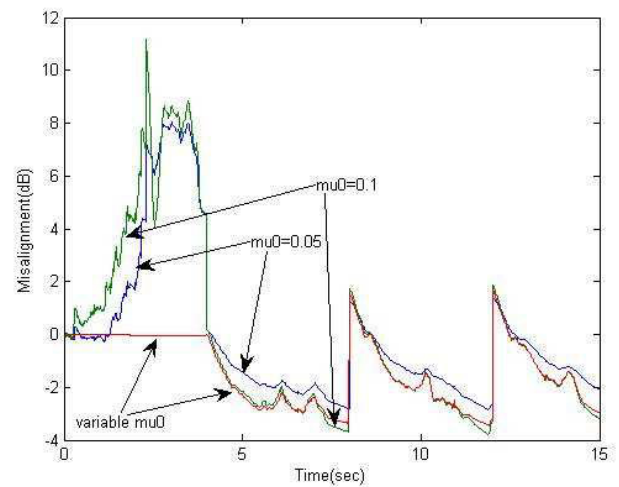


Fig. 7. Misalignment of PBFD-NLMS with dynamic (varying) feedback path (a) with constant step size (b) with variable step size. The results are the average of 40 executions in each of which the initial feedback path is the one depicted in Fig. 4 and the other feedback models are randomly generated.